

December 11, 2002

Dr. Andrew Rawicz School of Engineering Science Simon Fraser University Burnaby, British Columbia V5A 1S6

Subject: Post Mortem for ENSC 340: Wireless EMG Electrodes

Dear Dr. Rawicz:

The document enclosed with this letter, *Post Mortem for a Wireless EMG System*, is an outline of the technical and interpersonal experiences during ENSC 340. The goal of our project was to develop a system to sense, acquire and wirelessly transmit muscle activity data from a patient to a computer. Without wires limiting the patient's freedom of motion, this novel technology could revolutionize many aspects of rehabilitation, diagnosis and research.

In this document we present the current state of the device, deviations from the original specifications, and our future plans for the device. In addition, there is discussion on our budget, time management and personal experiences.

Wireless Medical Devices was formed in June of 2002 by four highly skilled and motivated Engineering Science students: Eric Chow, Aaron Ridinger, David Press, and Andrew Pruszynski. We look forward to hearing your comments on our proposal. Please feel free to contact us at wireless-medicaldevices@sfu.ca.

Sincerely,

Jedrzej (Andrew) Pruszynski Chief Executive Officer Wireless Medical Devices Enclosure: Proposal for Wireless EMG Electrodes

WIRELESS MEDICAL DEVICES

Project Team:

Eric Chow Dave Press Andrew Pruszynski Aaron Ridinger

Dr. Andrew Rawicz

Mr. Steve Whitmore

Submitted To:

Revision Number:

Revision Date:

December 13, 2002

1.0



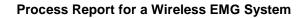
Table of Contents

1.0 - II	NTRODUCTION
2.0 - C	CURRENT DEVICE
2	2.1 - EMG Pad
3.0 – F	FUTURE PLANS
	3.1 - More TGEs93.2 - New Chipcon Transceiver93.3 - Miniaturization93.4 - Acquire Other Biological Signals103.5 - Increased Battery Life103.6 - Fully Independent Wireless EMG10
4.0 – P	PERSONAL EXPERIENCE10
4 4	4.1 – Andrew Pruszynski 10 4.2 – Eric Chow. 11 4.3 – David Press 11 4.4 – Aaron Ridinger. 12
5.0 - 1	TIMELINE
6.0 – E	BUDGET14
7.0 – 0	CONCLUSION
APPE	NDIX16
I I	Transmitter Microcontroller Code (Assembly)16Receiver Microcontroller Code (Assembly)23PC Software (C)32PC Software (Matlab)39



Acronyms

CMNR Common Mode Noise Rejection DAQ Data Acquisition ECG Electrocardiogram EEG Electroencephalogram EMG Electromyograph GUI Graphical User Interface iEMG Independent Electromyograph ISM Industrial, Scientific, and Medical I/O Input/Output MUX Multiplexer NRZ Non-Return to Zero PC Personal Computer PCB Printed Circuit Board PCI Peripheral Card Interface **RSSI** Received Signal Strength Indicator TGE Transmitter and Ground Electrode WMD Wireless Medical Devices





1.0 - Introduction

An Electromyograph is a recording of muscle activity used for rehabilitation, injury prevention and performance enhancement. Unfortunately, current systems rely on the use of restrictive wires and equipment that result in inaccurate and inconvenient diagnosis. Applying wireless communications principles to Electromyography (EMG) will lead directly to better diagnosis, research and rehabilitation. These advances have far-reaching implications for corporations, insurance agencies, athletes and patients.

Over the past 15 weeks, our group has been dedicated to producing a wireless EMG system that is capable of eliminating the restriction associated with current EMG products. Our product, iEMG, is shown in Figure 1.1.



Figure 1.1 – Our Wireless EMG System

We have faced an enormous challenge to design, implement and document an extremely complex system within tight budgetary and time constraints. Despite many long nights with difficult trials and tribulations, we have been able to present a system that meets every major technical objective we have set forth. It has been an exciting and very rewarding project, one that makes each of our team members extremely proud.



2.0 - Current Device

Figure 2.1 presents a block diagram of the system that we have produced in fulfillment of Engineering Science 340. We have produced a system that is capable of wirelessly acquiring muscle activity from four EMG pads simultaneously. Dr. Ted Milner, an expert EMG user, has confirmed these results.

Two EMG pads are associated with each TGE, which is responsible for providing ground and power to each system component, sampling the muscle activity data from the pads and transmitting the acquired data to the RS. The RS then receives the information, formulates the data word, and passes it to the PC. The software on the PC is then capable of displaying and recording the signals.

The following sections outline the current state of each sub-component in more detail.

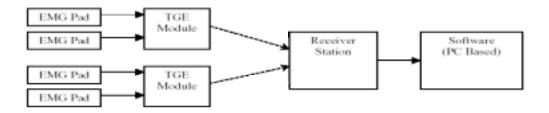


Figure 2.1 – Block Diagram of Wireless EMG System

2.1 – EMG Pad

Dr. Ted Milner of Kinesiology who has been manufacturing the devices for his research for several years provided the EMG pads. These pads are capable of acquiring the EMG data, amplifying to useful amplitudes and proving the signal at the output. We had initially stated in our Design Spec that we planned to run the pads off a +/- 3V supply, which we hoped to produce using a stack of four hearing aid batteries. We also knew that they needed a ground referenced to elsewhere on the subject's body to yield correct operation. However, we discovered that these pads required an input of +/-5V (even though all the components in the pad should have been able to run off lower voltages, which we were never able to explain).



2.2 – TGE Module

Each TGE module is capable of sampling and transmitting the muscle activity signal from two EMG pads at a rate high enough to ensure that no data significant data is lost. A block diagram of the TGE is presented in Figure 2.2.

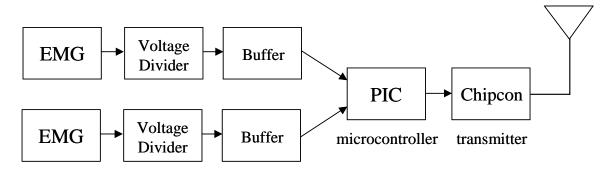


Figure 2.2 – Block Diagram of the TGE Module

TGE Hardware

As mentioned, we initially planned on using a stack of hearing aid batteries to power the TGE. However, after discovering our need a total of 10V, we decided that would simply require too many hearing aid batteries. Thus we decided to use a DC-DC voltage converter and a lower voltage battery. We decided on a 3V lithium cell, which could source enough current to run the EMG pads at over triple its own voltage, while still having sufficient voltage to run the Chipcon transmitter and PIC microcontroller (which require 2.7-3.3 Volts).

When we ran the power supply system as described above, we found that the voltage converter drew enormous current spikes from the battery, which caused a voltage swing of about 0.2 Volts in the battery's output. This proved to be too much variation for the PIC to run properly. Thus, we decided to draw the power for the PIC and Chipcon from the 10V supply through a 3.3V regulator. This was extremely power inefficient since the Chipcon draws more current than all of the EMG hardware combined, but we faced no other options short of purchasing more DC-DC converters to step the voltage down from 10V to 3.3V.

This method now allowed us to use batteries that supplied less than 3V (since the Maxim DC-DC converters we used accepted supply voltages as low as 1.8V). We then decided to produce one TGE running off the 3V lithium cells we had already bought, and another off of a pair of rechargeable AAA Ni-MH batteries. The complete TGE including two EMG pads drew 225 mA at a supply voltage of 2.8V, and this current requirement increased as the input voltage to the DC-DC converter decreased. We found that a single lithium cell could run the TGE for 6 hours continuously, while the 2 AAA's ran in for slightly over 2.5 hours.



Several hardware components were designed to adjust the EMG signal before sending it to the PIC Microcontroller for A/D conversion. The EMG signal varied between +10 and 0 volts, whereas the input to the PIC A/D converter needed to be between 3.3 and 0 volts. A simple 2-resistor voltage divider was added to vary the EMG signal between 3.3 and 0 volts, and a buffer was added before the PIC A/D input to prevent the converter from loading the circuit. The buffer was constructed using an OP-AMP in a negative feedback configuration. Initially a generic TLO72 opamp chip was used, but we found that the negative rail wasn't close enough to 0 volts, the negative power supply. To ensure the complete range down to zero volts, a rail-to-rail opamp was used.

We also faced some choices with regards to the transmitter antenna. After experimenting with various loops of wire, as well as integrated helical and loop antennas from Antenna Factor, we decided on a small helical antenna called the Antenna Factor JJB.

TGE Firmware

The firmware running on the TGE PIC is much the same as we had initially planned. Essentially, it samples the two A/D channels once per millisecond, and sends the samples to the Receiver Station.

We initially had hoped to use NRZ format data encoding, which allowed a maximum data rate of 76.8 kB/s. This allowed us to send every data sample twice, with a checksum, to reduce data errors. We also needed to send an identifier byte every millisecond before sending a set of data samples so the receiver would be able to synchronize to the incoming data stream. We found that errors in this start byte were much more catastrophic than in the data itself. Thus, the redundant data did little to help the overall sample error rate. The data rate wasn't high enough to send the samples twice in two separate packets with separate identifier bytes.

Thus, we decided to switch to Manchester encoding, which offered a lower data rate of 38.4 kB/s, but higher receiver sensitivity and thus fewer bit errors. Since each data sample was only sent once, there was no need for checksums, so we could just barely fit each packet into the allotted 1 millisecond time slot.

2.3 – Receiver Station

The RS is capable of receiving data from up two TGE modules, formulating the correct data structure and communicating this to the PC. A block diagram of the RS is presented in Figure 2.3.

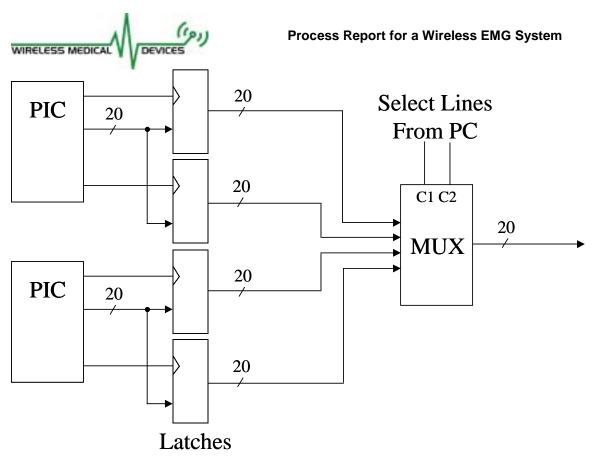


Figure 2.3 – Block Diagram of the Receiver Station

Receiver Firmware

The receiver station firmware is very similar to that described in the Design Specification. It syncronizes its USART to the incoming data by looking for the packet identifier byte. It then simply reads the incoming data, reads the A/D conversion from the Chipcon's RSSI pin, and forms the two output words (one for each sample. Each of these 20-bit data words is then latched into a set of D flip-flops. These latches ensure that the data is kept constant while the microcontroller switches between the two EMG Channels

One minor deviation from our original plans was the format of the output word, which is shown below in Figure 2.4. The incrementing ID bits are simply incremented by the PIC every time it updates the output word. This was necessary since the PC oversamples these output words, so it can simply compare the top nibble of every word it reads, and disregard the word if the incrementing ID is the same as the previous one from that particular EMG channel.



20-Bit Data							
4 Bits	12 Bits	4 Bits					
Incrementing ID	EMG Data	Signal Strength					
Figure 2.4 – Format of Output Word							

The output of the latches is connected to multiplexing circuitry that is controlled by the PC DIO Card for use by the software.

We chose to build the RS using spaghetti board rather than design a PCB to save time and money. We felt that a multi-layer PCB would be more difficult to fix if we discovered problems, and when we change the design of the receiver station to handle more TGEs the PCB would have to be redesigned anyways.

The receive side microcontroller source code is presented in the Appendix.

2.4 – PC Software

The PC software serves three major purposes. First, it allows the user to graphically observe the incoming data in real-time. Secondly, the incoming data can be recorded for future analysis. Lastly, some Matlab code was written to allow the import and observation of the acquired data signal.

Real-time graphical observation allows the user to correctly setup the EMG electrodes by ensuring correct pad placement and amplification. In addition, the user is shown the signal strength indicator (via RSSI) from each of the transmitting TGEs. This visual representation of receive signal strength lets the operator decide if the incoming signal strength is enough to ensure data consistency.

After the system has been verified graphically and the user is satisfied with the experimental setup, the data acquisition feature can be used to save muscle activity data. When the user begins data acquisition, the system will record the data from each EMG pad into an individual binary data file. The code has been written in such a way that ensures that no data points are lost and that no data points are saved twice.

The Matlab code was written to take advantage of the pre-fabricated GUI interface. More importantly, the ability to import our data files into Matlab is extremely important for the end users who will most likely be performing their data analysis within this software environment. Since our sampling at the TGE is very synchronous, we can provide the user with an accurate time-scale for the data stream. In addition, we can guarantee that this time scale applies to all the EMG signals recorded in each trial. These are very important features for the user.

We initially planned on a windows based GUI application for our PC software but after looking into the requirements and talking with people who have done similar programs, we decided that for this project a windows based GUI would not work. One of the main



reasons was to have a fast enough sampling time, we had to run the program in DOS because there was too much overhead for the API in windows. To be able to operate in windows, it is estimated that it would take an entire semester of work to write the appropriate device drivers and other software.

The source code for the C-based application software and the Matlab file for data analysis are included in the Appendix.

3.0 – Future Plans

The future for this product is extremely bright. It is ahead of the competition in terms of technology and could be produced for a much lower product price. In order to improve our market position and increase our technological advantage, there are several developments we are planning to make. The following sections outline these changes.

3.1 – More TGEs

Our most pressing issue is to expand the number of TGEs we currently have built. This does not require a redesign of our system, it simply requires manual labour and money to assemble more units. We would also have to expand the receiver station to handle the additional incoming data. The software is already designed to handle more TGE units. By making all the additional hardware, we will be capable of operating a maximum of 8 TGEs supporting up to 16 EMG pads without any significant system design changes.

3.2 – New Chipcon Transceiver

Chipcon, our supplier of wireless ISM band transceivers has just announced the release of a new transceiver. This product will be able to handle a higher data rate which would allow us to connect more EMG pads to a single TGE or send each sample twice for redundancy and error checking. The new transceiver is also designed specifically for narrow-band operation. This would allow us to fit more TGEs onto the 915MHz ISM band.

3.3 – Miniaturization

A critical body of work remains to place the design onto a PCB. We decided to avoid this for the purpose of this project to maximize our ability to debug the product and save time and money. Designing a PCB would have many significant effects on the product. Most importantly it would reduce the size and weight of the product. We estimate that a final PCB of the TGE would create a final size of 1.5" by 1.5". A design for the RS would also create a more compact and reliable package. Product miniaturization is critical to creating an unobtrusive and high quality product.



3.4 – Acquire Other Biological Signals

There are many other biological signals that fall within the same characteristics as EMG in terms of frequency range. Our product has been designed from the very beginning to be capable of handling these other biological signals. We can transmit any signal from DC to 500 Hz, and both ECG and EEG are much lower than this limit. We have yet to test this feature and it would be extremely interesting and important to develop our ability to transmit ECG, EEG, and other patient monitoring signals via the same hardware setup.

3.5 – Increased Battery Life

Our current battery life of 2.5 hours on two rechargeable NiMH batteries and 6 hours on one non-rechargeable lithium is appropriate for EMG data acquisition applications. However, as our system is adapted to other signals, we need to investigate increasing this battery life to 24 hours on rechargeable batteries. There are several options that must be investigated. First, a different hardware solution on the TGE could eliminate waste due to heat by eliminating voltage regulators. We could use two separate DC-DC converters, one to produce 10V and the other to produce 3.3V. This would cut the current consumption of the TGE by a factor of two, more than doubling our battery lifetime. Secondly, there exist proprietary battery technologies that may be better suited in terms of power, size and weight to deliver power to the system.

3.6 – Fully Independent Wireless EMG

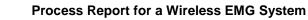
The initial goal of our system was to have absolutely no wires on the body. Unfortunately, the pads that were provided by Dr. Ted Milner required an external ground to work properly because of the internal operation of a differential amplifier. Therefore, one major goal is to redesign the EMG pad such that it can be used without the TGE. In this setup the transmitting would be done from each EMG pad directly, eliminating all the wires on the system. Currently, Aaron Ridinger is investigating the opportunity to develop such an EMG pad as his undergraduate thesis.

4.0 – Personal Experience

4.1 – Andrew Pruszynski

Developing this project has been one of the most rewarding, enjoyable and often frustrating experiences of my education. I have learned many technical and interpersonal skills that I will undoubtedly use for the rest of my life.

From a technical point of view, I have combined all the knowledge that I have gathered from my coursework and coop experience. We have been able to create something from only an idea. I developed the C based software which built on my experiences while working in the Biomechanics Laboratory and Ballard. I designed and manufactured the mother of all spaghetti boards that required digital design knowledge and all the soldering skills and patience that have been developed over the past four years. More important





then any single discreet contribution to the project was the endless debugging to figure out what was wrong and how to fix it. This has taught me that what is wrong is often the most simple thing, so simple that hours may be spent rejecting it as a possibility.

We have completed a large and difficult task and I am extremely happy with the final outcome, the personal experience associated with getting there and the technical knowledge that I have gained.

4.2 – Eric Chow

This project has shown me that many hours of research and development must go into a product in order to ensure a high quality end result. The project required us to work on all aspects of a product design, including research, hardware/software design, assembly and testing, purchasing and finances, and documentation.

The technical skills I have learned from other courses and jobs enabled me to contribute to the technical design of our project. Notable skills included hardware design, radio frequency communications, and basic electronics laboratory skills.

My contribution to the team was primarily focused on the research of a suitable RF transmitter/receiver pair and the TGE hardware design. In addition, I worked on building the prototype and assisted in the microcontroller firmware development.

In working with Andrew, Dave, and Aaron, I have realized the importance of good communication within a group to ensure good team dynamics. Our weekly meetings helped keep the group on track, and although tasks were divided among us we made sure to that everyone was kept up to date on the status of the project.

I see our product as having great market potential as well as research potential, and I hope to continue work with this product and this group in the future.

4.3 – David Press

I found this project both incredibly frustrating and incredibly rewarding. I have gained many skills and experiences that will aid me throughout my career.

Perhaps the most valuable single thing I learned is that when working on a project of this magnitude, not everything can be perfect. There were many times near the beginning when I would spend many hours perfecting a small aspect of the project. Towards the end, I learned that sometimes 'good enough is good enough', which is a huge step for me as I am known as a bit of a perfectionist.

My main contribution to this project was the firmware and transmission protocols for transmitting the data wirelessly. This was the first time I had picked up the manual for a completely unfamiliar microcontroller, and needed to learn every minute detail and quirk of its operation. I feel much more comfortable that I could do the same again if need be. I



also gained a lot of experience in haggling and hounding parts suppliers for lower prices and rushed shipping. I had to communicate frequently with design engineers at Chipcon in Norway, which proved to be an interesting cultural and logistical challenge. Overall, I am very pleased that the enormous effort we put into this project early on allowed us to accomplish our ambitious goals with time left to spare at the end of the semester.

4.4 – Aaron Ridinger

By working on this project I have further developed my technical, problem solving and interpersonal skills. I enjoyed both the technical aspects and team dynamics of this project.

New the beginning of this project I learned the many different possibilities of interfacing a PC with external devices such as USB, PCI, ISA, Firewire, and made a decision on which would work best for our project based on function and price. By working on the PC software I re-familiarized myself with programming in C, and utilized the Matlab skills I gained through past course work. Near the completion of the project I designed the TGE hardware and assembled it, which required me to recall my soldering skills I learned in high school.

Through this project and other course work this semester, I have discovered that I really don't want to design IC chips, as I initially planned on when I started studying engineering, but rather work in an area developing products to meet certain needs and solve specific solutions. After completing this project I now have an interest in bio-medical engineering. In the future I plan on doing a directed studies course in the area of EMG and mostly likely a thesis on the redesign of the EMG pad to eliminate the ground reference strap.



5.0 – Timeline

		_				Sej	o 2002				Oct 2	2002				Nov 2	2002		Dec	c 2002
ID	Task Name	Start	End	8/25	9/1	9/8	9/15	9/22	9/29	10/6	6 10,	/13 10/2	0 10/2	7	11/3 1	1/10	11/17	11/24	12/1	1 12/8
1	Proposal	26/08/2002	13/09/2002]													
2	Proposal Completed	13/09/2002	13/09/2002			•	•													
3	Research	26/08/2002	30/09/2002																	
4	Material Collection	02/09/2002	25/10/2002																	
5	1st Progress Report Completed	08/10/2002	08/10/2002							٠										
6	Functional Specification	16/09/2002	14/10/2002			Ŀ,														
7	Functional Specification Completed	14/10/2002	14/10/2002								٠									
8	Initial Design Specification	20/09/2002	10/10/2002								כ									
9	Design Specifications Finalized	21/10/2002	21/10/2002									٠								
10	Initial Prototype Build	04/10/2002	14/11/2002																	
11	Design Specification	11/10/2002	01/11/2002							•										
12	Design Specification Completed	01/11/2002	01/11/2002																	
13	Prototype Testing	06/11/2002	25/11/2002																	
14	2nd Progress Report Completed	29/11/2002	29/11/2002															•	•	
15	Prototype Revision	21/11/2002	04/12/2002																	
16	Product Prototype Completed	04/12/2002	04/12/2002																٠	
17	Post Mortem Report	29/11/2002	16/12/2002																	
18	Final Documentation Completed	13/12/2002	13/12/2002																	•
19	Document and Website Maintanance	26/08/2002	13/12/2002																	

Figure 5.1 presents the original timeline as included in the project proposal.

Figure 5.1 – Original Gantt Chart

It is very interesting to note that we met each of our target milestone dates. We made a significant effort to be ahead of schedule because we feared a large drain on our exam performance if too much ENSC340 work was left into the final weeks as originally planned. Thus, most of the difficult work was done very early in November, with a functioning prototype existing three weeks earlier then predicted. This allowed us several weeks to debug the system and focus our attention on assembly and testing.



6.0 – Budget

We applied and received a total of \$1500 of funding from the Wighton Fund and the ESSEF. A condensed spreadsheet outlining our expenses over the course of the semester is presented in Table 6.1.

Date	Description	Cost (\$CDN)
12/07/2002	Batteries	\$20.13
12/07/2002	Batteries	\$11.43
11/28/2002	Antennas	\$50.03
11/30/2002	Op-amps, Voltage Regulators	\$16.00
11/27/2002	EMG connectors	\$3.37
11/19/2002	DC-DC converter, voltage step up	\$128.00
10/14/2002	Transceivers	\$329.60
11/06/2002	Chipcon shipping	\$177.14
10/21/2002	PCI I/O card	\$176.55
10/01/2002	PICs, Lynx Transmitter, Receiver	\$181.47
11/06/2002	Oscillators, PICs, transmitter, receiver, UV Eraser	\$266.97
10/17/2002	Chipcon initial shipping	\$17.79
11/08/2002	Oscillators, multiplexers, Flip-Flops, PICs, PC board	\$127.02
09/30/2002	Phone card	\$5.00
11/13/2002	Phone card	\$5.00
11/16/2002	PC Board, switches	\$17.14
11/07/2002	Batteries	\$37.02
	Total Expenses	\$1,569.66

Table 6.1 – Simplified Table of All Expenses

It should be noted that we would be well within out budget if not for an unnecessary shipping charge due to miscommunication with the Engineering Science Office Staff. This mistake cost us \$177 as our ordered product made several trips across the Atlantic Ocean. In addition, we compared competing transmitter technologies for a cost of \$200. We will also be able to return approximately \$300 worth of components back to the School of Engineering Science for future use. With these notes in mind, Table 6.2 presents the cost of producing the final prototype for the course.

Item	Unit Cost	Units	Total cost
Batteries	\$15.77	1	\$15.77
Batteries	\$7.86	1	\$7.86
Batteries	\$9.97	1	\$9.97
PC Board	\$5.99	2	\$11.98
Switches	\$2.99	1	\$2.99
PCI-I/O Card	\$142.00	1	\$142.00
20MHz Oscillator	\$1.94	4	\$7.76
Dual 4 input multiplexer	\$1.19	12	\$14.28
D Flip-Flop	\$1.39	12	\$16.68
28 pin PIC16C773	\$18.99	2	\$37.98
40 pin PIC16C774	\$23.48	2	\$46.96

WIRELESS MEDICAL	Process	s Report for a	Wireless EMG System
PC Board	\$10.53	1	\$10.53
8MHz Oscillator	\$1.94	4	\$7.76
Transceivers CC1000PP 868MHz	\$64.00	4	\$256.00
DC-DC converter, voltage step up	\$56.00	2	\$112.00
EMG female connectors	\$1.27	1	\$1.27
EMG male connectors	\$1.67	1	\$1.67
Op-amp 7805UC??	\$4.99	1	\$4.99
Voltage Regulator LMC660CN???	\$4.49	2	\$8.98
Antenna 916MHz 1/4 wave	\$10.18	2	\$20.36
Antenna mini 7mm, 916MHz	\$3.16	2	\$6.32
Battery Holder	\$2.75	2	\$5.50
Batteries	\$9.98	1	\$9.98
Batteries	\$2.59	1	\$2.59
Batteries	\$14.99	1	\$14.99
Total Component Expenses			\$777.17

 Table 6.2 – Single Prototype Cost

We were able to produce a very complicated system without going significantly over budget. In fact, if not for an unexpected shipping cost and an extended evaluation of competing technologies, we would be well within our budgetary constraints.

7.0 – Conclusion

The past semester has been difficult, frustrating, tiring and most importantly rewarding for all the members of WMD. We have faced an enormous challenge to design, implement and document an extremely complex system within tight budgetary and time constraints. Despite many long nights with difficult trials and tribulations, we have succeeded. We now look into the future to see how to further improve our device and transform it from a project to a product.



Appendix

Transmitter Microcontroller Code (Assembly)

	p=16c773 <p16c773.inc></p16c773.inc>		list dire processor				-			5
CONFIG	CP OFF &	WDT ON &	BODEN ON	æ	PWRTE	ON &	RC	OSC &	VBOR	25

; '__CONFIG' directive is used to embed configuration data within .asm file. ; The lables following the directive are located in the respective .inc file. ; See respective data sheet for additional information on configuration word.

;**** VARIABL	E DEFINI	TIONS	
w_temp	EQU	0x70	; variable used for context saving
status_temp	EQU	0x71	; variable used for context saving
LAST_RES_0L LAST_RES_0H	EOU	EQU 0x73	0x72
LAST_RES_1L	EOU	0x73 0x74	
LAST_RES_1H	EQU	0x75	
OUR_STAT	EQU	0x76	; bit0 = done A/D, bit1 = last timer type, bit2 = calc
bytes out			
	TIOU	077	
w_prog_status byte_to_write		0x77 0x78	
num_bytes_writ		EQU	0x79
next_byte_out		$\tilde{0x7A}$	
dummy	EQU	0x20	
dummy2	EQU	0x21	
byte0 byte1	EQU EQU	0x22 0x23	
byte2	EOU	0x23 0x24	
byte3	EQU	0x25	
checksum	EQU	0x26	
out0	EQU	0x27	
out1	EQU	0x28	
out2	EQU	0x29	
out3	EQU	0x2A	
num_bytes_writ	ten_2	EQU	0x2B
w_temp_2	EQU	0x2C	
status_temp_2	ЕÕП	0x2D	
			_
DONE_AD	Ţ.	EQU	0 1
LAST_TIMER_TYP CALC_BYTES_OUT		EQU 2	
PREAMBLE_MODE		3	
SEND_BYTE	-2-	EQU	4
IS_ZERO		EQU	5
SEND_FILLER		EQU	6
t70us		EQU	0 1
t930us		EQU	1
;*********			* * * * * * * * * * * * * * * * * * * *
	ORG	0x000	; processor reset vector
	clrf	PCLATH main	; ensure page bits are cleared ; go to beginning of program
	goto	1110 111	, 30 co pedimind or brodram
	ORG	0x004	; interrupt vector location
	movwf	w_temp	
	movf	STATUS,	w ; move status register into W register

Process Report for a Wireless EMG System WIRELESS MEDICAL DEVICES movwf status_temp ; save off contents of STATUS register isr bsf STATUS, RPO ; page 1 btfss INTCON, TOIF goto int_was_USART ;;; int for timer btfss OUR_STAT, LAST_TIMER_TYPE goto was_70us ; last timer was 930 us bcf STATUS, RP0 ; page 0 movlw 0xEE movwf TMR0 ; set timer to overflow in 70 us bsf PORTA, 2 bsf ADCON0, CHS0 ; set next A/D to ch1 movf ADRESH, W ; get ch0 result movwf LAST_RES_OH bsf STATUS, RPO ; page 1 movf ADRESL, W movwf LAST_RES_0L bcf OUR_STAT, LAST_TIMER_TYPE ; last timer now was 70! goto finish_timer_isr was_70us bcf STATUS, RPO ; page 0 movlw 0x24 movwf TMR0 ; set timer to overflow in 930 us bcf ADCON0, CHS0 ; set next A/D to ch0 ; get ch1 result movf ADRESH, W movwf LAST_RES_1H bsf STATUS, RPO ; page 1 movf ADRESL, W LAST_RES_1L movwf OUR_STAT, LAST_TIMER_TYPE OUR_STAT, CALC_BYTES_OUT bsf ; last timer was 930 bsf finish_timer_isr bcf INTCON, TOIF ; reset the timer0 interupt flag bcf STATUS, RPO ; page 0 ADCON0, GO_DONE ; start A/D conversion bsf btfsc OUR_STAT, LAST_TIMER_TYPE end_isr goto ; last timer was 930 us, update the out0..out3 movf byte0,W movwf out0 movf byte1,W movwf out1 byte2,W movf movwf out2 bcf PORTA, 2 btfsc OUR_STAT, PREAMBLE_MODE end_isr goto



movlw 0x01 movwf num_bytes_written

goto end_isr

int_was_USART

bcf STATUS, RPO ; page 0 btfss OUR_STAT, PREAMBLE_MODE goto send_data send_out_preamble incf num_bytes_written, F movf num_bytes_written, W sublw 0xFF btfsc STATUS, Z goto end_preamble movlw 0x55 movwf TXREG goto end_isr end_preamble bcf OUR_STAT, PREAMBLE_MODE movlw 0x55movwf TXREG movlw 0x00movwf num_bytes_written bsf OUR_STAT, SEND_FILLER clrf num_bytes_written goto end_isr send_data movlw 0x80 num_bytes_written, 1 btfsc movf out0, W btfsc num_bytes_written, 2 movf out1, W num_bytes_written, 3 btfsc movf out2, W btfsc num_bytes_written, 4 movlw 0x55 write_to_txreg movwf TXREG bcf STATUS, C btfss num_bytes_written, 4 rlf num_bytes_written, F goto end_isr ;;;;;;;;; END OF ISR CODE;;;;;;;;; end_isr movf status_temp,w ; retrieve copy of STATUS register movwf STATUS ; restore pre-isr STATUS register contents movf w_temp, w retfie main ;;;;;; setup ;;;;;;;;;; STATUS, RP1 STATUS, RP0 bcf ; access page 1 bsf num_bytes_written clrf movlw $0 \times 0 \frac{1}{8}$ OUR_STAT movwf movlw 0x55 next_byte_out movwf 0x8D ; setup analog/digital IO PA0,PA1 analog movlw movwf ADCON1

WIRELESS MEDIC		(ig)		Process Report for a Wireless EMG System
	movlw movwf	0x03 TRISA	;	PA7PA2 output PA0, PA1 input
	movlw movwf	0x00 TRISB	;	PORTB outputs
	movlw movwf	0x50 TRISC	;	PC 6,4 input, rest output
for timer0, pr	movlw escaler movwf	0x02 to timer0, 1:8 OPTION_REG		pull ups enabled, int on rise edge, internal clock escaler (Fosc/32)
	movlw movwf	0x40 SSPSTAT	;	initialize SSPSTAT
	movlw movwf	0x32 TXSTA	;	initialize USART
	bsf	PIE1, TXIE	;	enable USART transmit interupt
	bcf	STATUS, RPO	;	access page 0
	movlw movwf	0x80 RCSTA		
	movlw movwf	0x30 SSPCON	; ;	enable SPI! must be after SSPSTAT has been written
	movlw movwf	0x81 ADCON0	;	A/D TOsc/32, ANO, No Conversion Complete, On
	movlw movwf	0x55 TXREG	;	put something in USART tx reg
	call	config_CC1000_	гх	
	movlw movwf	0xE0 INTCON	;	global interupt on, , timer0 int on, , ,
loop	btfss goto	OUR_STAT, CALC_ loop	_B?	TES_OUT
; just got out				ate the next message bytes ; page 0
;	movf	0x0F byte0 LAST_RES_0L, W	;	REMOVE THIS!!!
;	movlw movwf	0x34 bytel	;	REMOVE THIS!!!
ï	movf movlw andlw movwf movf	0x0F byte2	;	REMOVE THIS!!!
;	movlw movwf	LAST_RES_1L, W 0x78 byte3		REMOVE THIS!!!
; make byte 0	swapf	byte0, F		
	swapf andlw iorwf	bytel, W 0x0F byte0, F		
; make byte 1				

WIRELESS MEDICAL DEVICES swapf bytel, F 0xF0movlw bytel, F andwf movf byte2, W andlw $0 \times 0 F$ iorwf bytel, F ; make byte 2 movf byte3, W movwf byte2 end_calc bcf OUR_STAT, CALC_BYTES_OUT goto loop w_prog_addr movwf byte_to_write movf STATUS, W movwf w_prog_status STATUS, RPO STATUS, RP1 bcf bcf ; page 0 bcf PORTC, 2 ; clear PALE movf w_prog_status, W STATUS movwf movf byte_to_write, W w_prog_data ;;; writes a byte to prog CC1000 thru SPI movwf byte_to_write movf STATUS, W movwf w_prog_status ; save the current status STATUS, RPO STATUS, RP1 bcf ; page 0 bcf movf byte_to_write, W movwf SSPBUF ; page 1 ; wait for the byte to be written to SPI bsf STATUS, RPO wait_for_SPI_0 btfss SSPSTAT, BF goto wait_for_SPI_0 bcf STATUS, RPO ; page 0 bsf PORTC, 2 ; set PALE high movf w_prog_status, W movwf STATUS return r_prog reads a byte from CC1000 thru SPI ;;;;; returns byte in W reg ;;;;; movf STATUS, W w_prog_status ; save the current status movwf STATUS, RP1 STATUS, RP0 bcf bsf ; page 1 bsf TRISC, 5 ; set PC5 (Data out) to input bcf STATUS, RPO ; page 0 movwf SSPBUF ; write random crap from W bsf STATUS, RPO ; page 1 wait_for_SPI_1 btfss ; wait for the byte to be written to SPI SSPSTAT, BF

WIRELESS MEDICAL DEVICES goto wait_for_SPI_1 TRISC, 5 ; set PC5 to output bcf w_prog_status, W movf STATUS movwf return wait_500us clrf dummy wait1 incf dummy STATUS, Z btfss goto wait1 return ,,,,,,,,,,,,,,,,,,,,,, config_CC1000_TX ; make the transmit wake up later than the rx dummy2 wait_500us clrf wait3 call incf dummy2 btfss STATUS, Z goto wait3 movlw CC1000_MAIN_W call w_prog_addr movlw 0x3A w_prog_data call movlw CC1000_MAIN_W w_prog_addr 0x3B call movlw call w_prog_data wait_500us wait_500us call call wait_500us wait_500us call call wait_500us call CC1000_FREQ_2A_W movlw call w_prog_addr movlw 0x5B call w_prog_data movlw CC1000_FREQ_1A_W call w_prog_addr movlw 0xA3 call w_prog_data movlw CC1000_FREQ_0A_W call w_prog_addr movlw 0x13call w_prog_data movlw CC1000_FREQ_2B_W call w_prog_addr movlw $0 \times 5B$ call w_prog_data movlw CC1000_FREQ_1B_W call w_prog_addr movlw 0xA3 w_prog_data call CC1000_FREQ_0B_W movlw w_prog_addr 0x13 call movlw w_prog_data call CC1000_FSEP1_W movlw call w_prog_addr movlw 0x01 call w_prog_data CC1000_FSEP0_W movlw call w_prog_addr 0xAB movlw call w_prog_data



CC1000_CURRENT_W call w_prog_addr 0xF3 movlw w_prog_data call movlw CC1000_FRONT_END_W call w_prog_addr movlw 0x32 call w_prog_data CC1000_PA_POW_W movlw call w_prog_addr movlw 0×00 call w_prog_data CC1000_PLL_W movlw call w_prog_addr movlw 0×30 call w_prog_data movlw CC1000_LOCK_W call w_prog_addr movlw 0x10call w_prog_data movlw CC1000_MODEM2_W call w_prog_addr movlw 0xC2 call w_prog_data movlw CC1000_MODEM1_W call w_prog_addr movlw 0x6F ; was 13, keep at 6F w_prog_data call CC1000_MODEM0_W movlw call w_prog_addr 0x54 movlw call w_prog_data movlw CC1000_MATCH_W call w_prog_addr 0×10 movlw call w_prog_data movlw CC1000_FSCTRL_W call w_prog_addr movlw 0×01 w_prog_data call CC1000_PRESCALER_W movlw call w_prog_addr movlw 0×00 call w_prog_data CC1000_TEST6_W movlw call w_prog_addr movlw 0x10call w_prog_data movlw CC1000_TEST5_W call w_prog_addr movlw 0×08 call w_prog_data movlw CC1000_TEST4_W call w_prog_addr 0x3F movlw call w_prog_data CC1000_TEST3_W movlw call w_prog_addr 0×04 movlw w_prog_data CC1000_TEST2_W call movlw call w_prog_addr $0 \times 0 0$ movlw w_prog_data call CC1000_TEST1_W movlw call w_prog_addr 0x00movlw call w_prog_data CC1000_TEST0_W movlw

; set PA_POW to zero for calibration



	call	0x00 w_prog_data		
; begin calibr;	ation movlw call movlw call	CC1000_CAL_W w_prog_addr 0x66 w_prog_data		
	movlw call movlw call	CC1000_MAIN_W w_prog_addr 0xA1 w_prog_data		
	call call call call call	wait_500us wait_500us wait_500us wait_500us wait_500us		
	movlw call movlw call	CC1000_CURRENT_W w_prog_addr 0xF3 w_prog_data		
	movlw call movlw call	CC1000_CAL_W w_prog_addr 0xE6 w_prog_data		
wait2	clrf call incf btfss goto	dummy2 wait_500us dummy2 STATUS, Z wait2		
; end calibrat.	movlw call movlw call ion	CC1000_CAL_W w_prog_addr 0x66 w_prog_data		
	movlw call movlw call	CC1000_PA_POW_W w_prog_addr 0xFF w_prog_data		
	call	wait_500us		
	return			
	END		; directive	'end of program'

Receiver Microcontroller Code (Assembly)

	p=16c774 <p16c774.inc></p16c774.inc>		; list directive to define processor ; processor specific variable definitions
CONFIG	_CP_OFF & _WDT_ON	<u>م</u>	_BODEN_ON & _PWRTE_ON & _RC_OSC & _VBOR_25

; '__CONFIG' directive is used to embed configuration data within .asm file. ; The lables following the directive are located in the respective .inc file. ; See respective data sheet for additional information on configuration word.

;***** VARIABLE DEFINITIONS



w_temp status_temp RSSI DATA0 OUR_STAT	EQU EQU EQU EQU EQU	0x70 0x71 0x72 0x73 0x74	; variab	le used for le used for done A/D		
w_prog_status num_match_byte our_state byte_to_write	EQU S EQU EQU	0x75 EQU 0x77 0x78	0x76			
dummy dummy2	EQU EQU	0x20 0x21				
byte_num byte0 byte1 byte2 byte3 byte4 byte5 byte6 byte7	EQU EQU EQU EQU EQU EQU EQU EQU	0x22 0x23 0x24 0x25 0x26 0x27 0x28 0x29 0x2A				
checksum1 checksum2 checksum3 checksum4	EQU EQU EQU EQU	0x2B 0x2C 0x2D 0x2E				
num_times_wait	ed	EQU	0x2F			
in0 in1 in2 in3 in4 in5 in6 in7	EQU EQU EQU EQU EQU EQU EQU EQU	0x30 0x31 0x32 0x33 0x34 0x35 0x36 0x37				
out1B out1D out1A out2B out2D out2A counter header	EQU EQU EQU EQU EQU EQU EQU	0x38 0x39 0x3A 0x3B 0x3C 0x3D 0x3E 0x3F				
; OUR_STAT bit WAIT_FOR_SB DO_CALC sampla_bad samp2a_bad samp1b_bad samp2b_bad	EQU EQU EQU EQU EQU EQU	0 1 2 3 4 5				
; our_state wo WAIT_FOR_SYNC SYNC	ras	EQU EQU	0x04 0x08			
;*********	* * * * * * * *			* * * * * * * * * * * *	******	* * * * * * * * *
ŗ	ORG clrf goto	0x000 PCLATH		; processor ; ensure pag ; go to begi	reset ve Je bits a	ctor re cleared
	ORG movwf movf movwf	STATUS	w ;	move statu	urrent W s registe	ocation 'register contents er into W register of STATUS register
; isr code can ;;;;;;; BEGIN isr				call subrou	tine els	ewhere



int_was_USART

STATUS, RPO ; page 0

movf RCREG, W movwf btfsc goto DATAO our_state, 3 get_data

wait_sync

	bcf bcf	STATUS, RPO RCSTA, SPEN		; page 0 ; disable t	he USART	
start_count count_this	clrf	dummy				
count_cnis	incf	dummy,F				
; up!!! cant loc		nitial message	is all O		as a nop here, but or some reason!	it fucks things
	btfss goto	PORTC,7 count_this				
byte	btfss	dummy, 5	; must g	get thru th	is loop 64 times to	be the start
	goto	start_count				
	movlw movwf	SYNC_ our_state				
	clrf	OUR_STAT				
	nop					
	nop nop					
	nop					
	nop nop					
	nop nop					
	movlw	0x00				
gohere	movwf	dummy				
	incf btfss	dummy, F dummy, 3				
	goto	gohere				
	bcf movlw	RCSTA, CREN 0x90	; clear	an overrun	if there was one	
	movwf		; turn c	on USART		
	goto	end_isr				
get_data						
	movf btfss	DATAO, W OUR_STAT, WAIT_	FOD CD			
	goto	get_data_byte	_10K_00			
; check if its		byte num_times_waite	d E			
	btfsc	num_times_waite	ed, 3			
row, we're scr	goto ewed up		; iI we'	ve looked :	for the start byte	8 times in a
	sublw btfss	0x80 STATUS, Z				
	goto		; nope,	not a star	t byte	
; start byte						
	clrf bcf	<pre>num_times_waite OUR_STAT, WAIT_</pre>				
	movlw movwf	0x01	011_02			
		byte_num				
	movf movwf	byte0, W in0				
						. ^

WIRELESS MEDICAL DEVICES movf bytel, W movwf in1 byte2, W movf movwf in2 bcf PORTA, 5 btfsc RSSI, 3 bsf PORTA, 5 swapf RSSI, W andlw 0×07 PORTE movwf movf out1B, W movwf PORTB movf out1D, W movwf PORTD bsf PORTC, 0 bcf PORTC, 0 movf out2B, W ; uncomment this after demo movwf PORTB movf out2D, W movwf PORTD bsf PORTC, 1 bcf PORTC, 1 bsf OUR_STAT, DO_CALC end_isr goto screwed 0x04 ;;;;;;old movlw ; our_state movwf ; 0x01 movlw ; movwf byte_num ; movlw 0x04;;;;; new our_state movwf OUR_STAT num_times_waited clrf clrf movlw 0x01 movwf byte_num end_isr goto ; we're not waiting for SB so its data get_data_byte ; W contains data btfsc byte_num,0 movwf byte0 btfsc byte_num,1 movwf byte1 btfsc byte_num,2 movwf byte2 bcf STATUS, C rlf byte_num, F byte_num, 3 OUR_STAT, WAIT_FOR_SB btfsc bsf goto end_isr ;;;;;;;;; END OF ISR CODE;;;;;;;;; end_isr ; retrieve copy of STATUS register ; restore pre-isr STATUS register contents movf status_temp,w movwf STATUS swapf w_temp,f ; restore pre-isr W register contents swapf w_temp,w

WIRELESS MEDIC		(in a state of the	Process Report for a Wireless EMG System
;;;;;;;;;;; ENI	retfie OF ISR	,,,,,,,,,,,,,,,,,,,	; return from interrupt ;;
main ;;;;;; setup ;	bcf bsf	; STATUS, RP1 STATUS, RP0	; access page 1
justified	movlw movwf	0x0E ADCON1	; setup analog/digital IO PAO analog, left
	movlw movwf	0x01 TRISA	; PA7PA1 output PA0, input
	movlw movwf movlw movwf movlw movwf	0x00 TRISB 0x00 TRISD 0x00 TRISE	; PORTE outputs ; PORTD outputs ; PORTE outputs, PE & PD general purpose I/O
	movlw movwf	0xD0 TRISC	; PC 7,6,4 input, rest output
for timer0, pr	movlw rescaler movwf	0x02 to timer0, 1:8 OPTION_REG	; pull ups enabled, int on rise edge, internal clock 3 prescaler (Fosc/32)
	movlw movwf	0x40 SSPSTAT	; initialize SPI
	movlw movwf	0x12 TXSTA	; initialize USART
	bsf	PIE1, RCIE	; enable USART receiver interupt
	bcf	STATUS, RPO	; access page 0
	movlw movwf clrf movlw movwf	0x04 our_state OUR_STAT 0x01 byte_num	
	movlw movwf	0x80 RCSTA	
	movlw movwf	0x30 SSPCON	; ; enable SPI! must be after SSPSTAT has been written
	movlw movwf	0x81 ADCON0	; A/D TOsc/32, ANO, No Conversion Complete, On
	call	config_CC1000_	_RX
	movlw movwf	0xC0 INTCON	; global interupt on, , timer0 int off, , ,
	movlw movwf	0x90 RCSTA	; enable cont receive on USART
loop			
	bcf btfss goto	STATUS,RP0 OUR_STAT, DO_C loop	; make sure we're on page 0 CALC
analyze_data			
	bcf movf), GO_DONE ; get ch0 result



	IIIOVWI	K551	
W	incf	counter, F	; get the header nibble ready, OF in
		0x0F counter, F	
	movf andlw movwf swapf		
		counter, W out1B, F	
	movf andlw movwf swapf	out1D	
	andlw	inl, W 0x0F out1D, F	
	movf andlw movwf		
		counter, W out2B, F	
	movf movwf	in2, W out2D	
end_calc			
	bsf bcf goto	ADCON0, GO_DON OUR_STAT, DO_C loop	E ; start next A/D conversion ALC
,,,,,,,,,,,,,,,,,,,,	; SUBROU	JTINES ;;;;;;;;;;	;;;;
;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;	;;;;;;;;	;	
w_prog_addr	movwf movf movwf	byte_to_write STATUS, W w_prog_status	
	bcf bcf	STATUS, RPO STATUS, RP1	; page 0
	bcf	PORTC, 2	; clear PALE
	movf movwf movf	w_prog_status, STATUS byte_to_write,	
w_prog_data			;;; writes a byte to prog CC1000 thru SPI
	movwf movf movwf	byte_to_write STATUS, W w_prog_status	
	bcf bcf	STATUS, RPO STATUS, RP1	; page 0
	movf movwf	byte_to_write, SSPBUF	W
wait_for_SPI_0	bsf btfss goto	STATUS, RPO SSPSTAT, BF wait_for_SPI_0	; page 1 ; wait for the byte to be written to SPI
	bcf bsf	STATUS, RPO PORTC, 2	; page 0 ; set PALE high
	movf	w_prog_status,	W

WIRELESS MEDIC		((e))	Process Report for a Wireless EMG S
,,,,,,,,,,,,,,,,,,,	<pre>movwf return ;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;</pre>	STATUS	
r_prog	;;;;; ;;;;; movf	returns byte ir STATUS, W	-
	movwf bcf	w_prog_status STATUS, RP1	; save the current status
	bsf	STATUS, RPO	; page 1
	bsf		; set PC5 (Data out) to input
	bcf	STATUS, RPO	; page 0
wait_for_SPI_1		SSPBUF STATUS, RPO SSPSTAT, BF	<pre>; write random crap from W ; page 1 ; wait for the byte to be written to SPI</pre>
	goto bcf	<pre>wait_for_SPI_1 TRISC, 5</pre>	; set PC5 to output
	movf movwf	w_prog_status, STATUS	
,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,,	return ;		
lock_filt	movlw call movlw call return	CC1000_MODEM1_v w_prog_addr 0x7F w_prog_data	4
unlock_filt	movlw call movlw call return	CC1000_MODEM1_v w_prog_addr 0x6F w_prog_data	7
;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;	;;;		
wait1	clrf incf btfss goto return	dummy dummy STATUS, Z waitl	
;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;;	;;;		
config_CC1000_	RX		
	movlw call movlw call	CC1000_MAIN_W w_prog_addr 0x3A w_prog_data	
	movlw call movlw call	CC1000_MAIN_W w_prog_addr 0x3B w_prog_data	
	call call call call call	wait_500us wait_500us wait_500us wait_500us wait_500us	
	movlw call movlw call movlw	CC1000_FREQ_2A_ w_prog_addr 0x5B w_prog_data CC1000_FREQ_1A_	



call w_prog_data CC1000_FREQ_0A_W movlw call w_prog_addr 0×00 movlw w_prog_data call CC1000_FREQ_2B_W movlw w_prog_addr call movlw 0x5B w_prog_data call movlw CC1000_FREQ_1B_W call w_prog_addr movlw 0xA0 call w_prog_data movlw CC1000_FREQ_0B_W call w_prog_addr movlw 0x00call w_prog_data movlw CC1000_FSEP1_W call w_prog_addr movlw 0×01 call w_prog_data movlw CC1000_FSEP0_W call w_prog_addr movlw 0xAB call w_prog_data movlw CC1000_CURRENT_W call w_prog_addr 0x8C movlw call w_prog_data CC1000_FRONT_END_W movlw call w_prog_addr movlw 0×32 w_prog_data call CC1000_PA_POW_W movlw call w_prog_addr 0×00 movlw call w_prog_data CC1000_PLL_W movlw call w_prog_addr movlw 0x30 call w_prog_data movlw CC1000_LOCK_W call w_prog_addr movlw 0×10 call w_prog_data movlw CC1000_MODEM2_W call w_prog_addr movlw $0 \times C2$ call w_prog_data movlw CC1000_MODEM1_W call w_prog_addr movlw 0x6F call w_prog_data CC1000_MODEM0_W movlw call w_prog_addr movlw 0x54w_prog_data call CC1000_MATCH_W movlw w_prog_addr 0x10 call movlw call w_prog_data movlw CC1000_FSCTRL_W call w_prog_addr movlw 0x01 call w_prog_data movlw CC1000_PRESCALER_W

; set PA_POW to zero for calibration

WIRELESS MEDIC		(iq))	Ρ
	call movlw call	w_prog_addr 0x00 w_prog_data	
	movlw call movlw call	CC1000_TEST6_W w_prog_addr 0x10 w_prog_data	
	movlw call movlw call	CC1000_TEST5_W w_prog_addr 0x08 w_prog_data	
	movlw call movlw call movlw call movlw call movlw call movlw call movlw call movlw call movlw call movlw call	CC1000_TEST4_W w_prog_addr 0x3F w_prog_data CC1000_TEST3_W w_prog_addr 0x04 w_prog_data CC1000_TEST2_W w_prog_addr 0x00 w_prog_data CC1000_TEST1_W w_prog_addr 0x00 w_prog_data CC1000_TEST0_W w_prog_addr 0x00 w_prog_addr 0x00 w_prog_addr 0x00 w_prog_addr 0x00	
; begin calibr	ation movlw call movlw call movlw call movlw	CC1000_CAL_W w_prog_addr 0x66 w_prog_data CC1000_MAIN_W w_prog_addr 0x11	
	call call call call call call movlw	<pre>w_prog_data wait_500us wait_500us wait_500us wait_500us wait_500us CC1000_CURRENT_W</pre>	
	call movlw call	w_prog_addr 0x8C w_prog_data	
	movlw call movlw call	CC1000_CAL_W w_prog_addr 0xE6 w_prog_data	
wait2	clrf call incf btfss goto	dummy2 wait_500us dummy2 STATUS, Z wait2	
; end calibrat		CC1000_CAL_W w_prog_addr 0x66 w_prog_data	
	return END		; di

; directive 'end of program'



PC Software (C)

		/
<pre>#include #include #includ</pre>		<pre>h> > s.h> h>h> > h> cs.h> ********</pre>
<pre>#define base #define porta #define portb #define portc #define ctrl</pre>	0xfff4 base+0 base+1 base+2 base+3	
#define #define #define	DIAG ACQ QUIT	1 2 3
<pre>#define #define #define #define #define #define #define #define #define #define #define</pre>	Y_RES X_RES XAXSTR XAXEND XSTRT XEND RECLEAD YOFFSET XOFFSET	
#define #define #define #define	XMIN XMAX YMIN YMAX	0 640 0 480
<pre>#define #define #define #define #define #define #define #define #define #define</pre>	PAD8 PAD7 PAD6 PAD5 PAD4 PAD3 PAD2 PAD1	8 7 6 5 4 3 2 1
<pre>#define #define #define #define #define #define #define #define #define #define</pre>	YMIN8 YMIN7 YMIN6 YMIN5 YMIN4 YMIN3 YMIN2 YMIN2 YMIN1	0 60 120 180 240 300 360 420
<pre>#define #define #define #define #define #define #define #define #define #define</pre>	YMAX8 YMAX7 YMAX6 YMAX5 YMAX4 YMAX3 YMAX2 YMAX1	59 119 179 239 299 359 419 479
<pre>#define #define #define #define #define #define</pre>	XAXIS8 XAXIS7 XAXIS6 XAXIS5 XAXIS4	30 90 150 210 270

```
WIRELESS MEDICAL
                         DEVICES
#define
                   XAXIS3
                            330
#define
                            390
                   XAXIS2
                           450
#define
                  XAXIS1
FUNCTION PROTOTYPES
**********************************
void init(void);
int intro(void);
void data_diag(void);
void data_acq(void);
unsigned int truncate(unsigned long int);
void rt_graph(int *x_last,int *y_last, int ymin, int ymax, int xaxis);
void rt_sigstr(unsigned long int, int);
void draw_rectangles(void);
void draw_lines(void);
/********
GLOBALS
FILE *fp_1, *fp_2, *fp_3, *fp_4, *fp_5, *fp_6, *fp_7, *fp_8;
unsigned long int ms_data = 0, ls_data = 0, data = 0;
unsigned long int last_data_1, last_data_2, last_data_3, last_data_4, last_data_5,
last_data_6, last_data_7, last_data_8;
int empty_1 = 1, empty_2 = 1, empty_3 = 1, empty_4 = 1, empty_5 = 1, empty_6 = 1, empty_7
= 1, empty_8 = 1;
int x_8 = XSTRT, x_7 = XSTRT, x_6 = XSTRT, x_5 = XSTRT, x_4 = XSTRT, x_3 = XSTRT, x_2 =
XSTRT, x_1 = XSTRT;
int y_8 = 30, y_7 = 90, y_6 = 150, y_5 = 210, y_4 = 270, y_3 = 330, y_2 = 390, y_1 = 450;
unsigned int short_data = 0;
int yaxis;
int mode = 0;
int input;
int mux_sel = 0x0;
int check;
int delay_sigstr = 0;
int gdriver = DETECT;
int gmode;
TEMPORARY GLOBALS
***************************
long int x = 0, y = 0;
unsigned long int test;
int tester=0;
main()
{
         init();
                            // initialization of IO Card and Files
         mode = intro();
         while(1)
         {
                   if(mode == DIAG)
                           data_diag();
                   else if(mode == ACQ)
                            data_acq();
                   else if(mode == QUIT)
                            exit(0);
                  mode = 0;
                  mode = intro();
         }
}
void init()
         // Initalize the DIO Control Register, Regular Mode, A,B,CH In
         outp(ctrl, 0x9A);
```



```
if((fp_8 = fopen("C:\\WMD\\emg1.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       if((fp_7 = fopen("C:\\WMD\\emg2.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       if((fp_6 = fopen("C:\\WMD\\emg3.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       if((fp_5 = fopen("C:\\WMD\\emg4.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       if((fp_4 = fopen("C:\\WMD\\emg5.dat", "wb+"))==NULL)
       {
              printf("Cannot open file.\n");
              exit(1);
       if((fp_3 = fopen("C:\\WMD\\emg6.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       if((fp_2 = fopen("C:\\WMD\\emg7.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       if((fp_1 = fopen("C:\\WMD\\emg8.dat", "wb+"))==NULL)
              printf("Cannot open file.\n");
              exit(1);
       }
}
int intro()
      printf("\n\n\n\n\n\n\n\n\n\n\n\n\n\n\n
printf("Please Select Your Mode: (d)iagnositc, (a)cquisition, (q)uit\n");
      while(mode == 0)
       {
              input = getch();
              if(input=='d')
              {
                     mode = DIAG;
                     printf("Entering Diagnostic Mode\n");
              else if (input == 'a')
              ł
                     mode = ACQ;
                     printf("Entering Acquisition Mode\n");
              ł
              else if (input == 'q')
                     mode = QUIT;
                     printf("Now Terminating, GoodBye");
                     delay(1000);
              }
              élse
                     printf("Invald Entry, Please Try Again\n");
      return mode;
}
void data_diag()
       ("Entering Diagnostic Mode, press any key to \texttt{Exit\n"});
       initgraph(&gdriver, &gmode, "\bgi");
```

```
WIRELESS MEDICAL
           if(graphresult() != grOk)
           {
                      printf("Error Opening Graphics Window.");
                      getch();
                      exit(1);
           }
           //labelling display
          outtextxy(XSTRT-42,XAXIS8, "EMG1");
outtextxy(XSTRT-42,XAXIS7, "EMG2");
outtextxy(XSTRT-42,XAXIS7, "EMG3");
outtextxy(XSTRT-42,XAXIS5, "EMG4");
outtextxy(XSTRT-42,XAXIS5, "EMG4");
outtextxy(XSTRT-42,XAXIS3, "EMG6");
outtextxy(XSTRT-42,XAXIS2, "EMG6");
outtextxy(XSTRT-42,XAXIS1, "EMG8");
outtextxy(XSTRT-42,XAXIS1, "EMG8");
           outtextxy(XSTRT-115, 5, "Sig_Str");
          outtextxy(XSTRT - 79, XAXIS8+28, "TGE1");
outtextxy(XSTRT - 79, XAXIS6+28, "TGE2");
outtextxy(XSTRT - 79, XAXIS4+28, "TGE3");
outtextxy(XSTRT - 79, XAXIS2+28, "TGE4");
           // draw initial y axis
           setcolor(1);
           int yaxis = 0 + YOFFSET;
           while (yaxis < 480)
           {
                      line(XAXSTR,yaxis,XAXEND,yaxis);
                      yaxis = yaxis+60;
           }
            // draw initial x axis
           line(XOFFSET,YMIN,XOFFSET,YMAX);
           // draw outline of signal strength boxes
           draw_rectangles();
           draw_lines();
           test = 0x0;
           while(!kbhit())
           {
                      ms_data = inpw(porta);
                      ls_data = (0xF0 & inp(portc)) >> 4;
ms_data = (ms_data << 4);
data = ((0x000FFFFF & (ms_data | ls_data)));
                      outp(portc, (0x3 & (mux_sel+1))) << 2); // sets the MUX to toggle to next
pad
                      if(mux_sel == 0x0)
                       {
                                 rt_graph(&x_8,&y_8,YMIN8,YMAX8,XAXIS8);
                                 rt_sigstr(data, PAD8);
                      }
                      else if (mux_sel == 0x2)
                       {
                                 rt_graph(&x_7,&y_7,YMIN7,YMAX7,XAXIS7);
                                 rt_sigstr(data, PAD7);
                      if (mux_sel == 0x1)
                       {
                                 rt_graph(&x_6,&y_6,YMIN6,YMAX6,XAXIS6);
rt_sigstr(data, PAD6);
                      else if (mux_sel == 0x3)
                                 rt_graph(&x_5,&y_5,YMIN5,YMAX5,XAXIS5);
                                 rt_sigstr(data, PAD5);
                      }
                      if(mux_sel<0x3)
                                 mux_sel++;
                      else
                                 mux sel = 0x0;
           }
           getch();
           closegraph();
void data_acq()
```

}

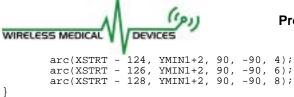
```
{ // begin data acquisition
        printf("Press any Key to Begin Data Acquisition\n");
        getch();
        printf("\n~~~~~Data Acquisition Started~~~~~\n");
        printf("\n\nPress Any Key to Stop\n");
        x = 0;
// begin data acquistion
        while(!kbhit())
                ms_data = inpw(porta);
                ls_data = (0xF0 & inp(portc)) >> 4;
                ms_data = (ms_data << 4);
data = ((0x000FFFFF & (ms_data | ls_data)));
                check = (0xF0000 & data) >> 16;
outp(portc, (0x3 & (mux_sel+1)) << 2); // sets the MUX to toggle to next pad outp(portc, (0x3 & (mux_sel+1)) << 2); // sets the MUX to toggle to next pa
                if(mux_sel == 0x0)
                {
                        if((check != last_data_8) || (empty_8 == 1))
                                short_data = truncate(data);
                                fwrite(&short_data, sizeof(short_data), 1, fp_8);
                                last_data_8 = check;
                                empty_8 = 0;
                        }
                else if (mux_sel == 0x2)
                        if((check != last_data_7) || (empty_7 == 1))
                        {
                                short data = truncate(data);
                                fwrite(&short_data, sizeof(short_data), 1, fp_7);
                                last_data_7 = check;
                                empty_7 = 0;
                        }
                else if (mux_sel == 0x1)
                        if((check != last_data_6) || (empty_6 == 1))
                        {
                                short_data = truncate(data);
                                fwrite(&short_data, sizeof(short_data), 1, fp_6);
                                last_data_6 = check;
                                empty_6 = 0;
                        }
                else if (mux_sel == 0x3)
                {
                        if((check != last_data_5) || (empty_5 == 1))
                        ł
                                short_data = truncate(data);
                                fwrite(&short_data, sizeof(short_data), 1, fp_5);
                                last_data_5 = check;
                                empty_5 = 0;
                        }
                if(mux_sel<0x3)
                        mux_sel++;
                else
                        mux_sel = 0x0;
        getch();
        printf("Please Move the Data (emgl.dat-emg8.dat) Files Before You Attempt to
Acquire More Data\n");
        printf("\n\nPress any Key to Continue...\n");
        getch();
}
unsigned int truncate(unsigned long int in_data)
        int out_data;
        in_data = (0x000FFF0 & in_data) >> 4;
        out_data = in_data;
```

WIRELESS MEDICAL

```
WIRELESS MEDICAL
       return out_data;
}
void rt_graph(int *x_last,int *y_last, int ymin, int ymax, int xaxis)
       short_data = ((truncate(data))/(Y_RES));
       setcolor(0);
       rectangle(*x_last,ymin,*x_last+RECLEAD,ymax);
       setcolor(2);
       line(*x_last, *y_last,*x_last+X_RES,ymax-short_data);
       setcolor(1);
       line(XAXSTR,xaxis,XAXEND,xaxis);
       if(*x_last <= XEND)
                *x_last = *x_last + 1;
       else
               *x_last = XSTRT;
       *y_last = ymax-short_data;
}
void rt_sigstr(unsigned long int in_data, int pad)
ł
       if(delay_sigstr < 500)
               delay_sigstr++;
       else
       {
               int sigstr, sigstr_last1 = 0, sigstr_last2 = 0;
               in_data = 16 - (in_data \& 0xF);
               sigstr = ((4*in_data)-18)*1.53;
               if (sigstr <= 0)
                       sigstr = 64;
               else if (sigstr > 64)
                       sigstr = 0;
               if(pad == PAD8 || pad == PAD7)
                       if(sigstr < 0)
                       sigstr = sigstr_last1;
else if (sigstr > 64)
                               sigstr = sigstr_last1;
                       else
                               sigstr_last1 = sigstr;
                       setfillstyle(0,0);
                       bar(XSTRT-89,YMAX8+34,XSTRT-86,YMIN8+29);
                       if (sigstr > 40)
                       {
                               setfillstyle(1,2);
                               bar(XSTRT-89,YMAX8+34-sigstr,XSTRT-86,(YMAX8+34));
                       else if (sigstr > 20)
                       {
                               setfillstyle(1,14);
                               bar(XSTRT-89,YMAX8+34-sigstr,XSTRT-86,(YMAX8+34));
                       élse
                       ł
                               setfillstyle(1,4);
                               bar(XSTRT-89,YMAX8+34-sigstr,XSTRT-86,(YMAX8+34));
                       }
               else if(pad == PAD6 || pad == PAD5)
                       if(sigstr < 0)
                       sigstr = sigstr_last2;
else if (sigstr > 64)
                               sigstr = sigstr_last2;
                       else
                               sigstr_last2 = sigstr;
                       setfillstyle(0,0);
                       bar(XSTRT-89,YMAX6+34,XSTRT-86,YMIN6+29);
                       if(sigstr > 40)
```

```
Process Report for a Wireless EMG System
WIRELESS MEDICAL
                                DEVICES
                                    {
                                                setfillstyle(1,2);
                                                bar(XSTRT-89,YMAX6+34-sigstr,XSTRT-86,(YMAX6+34));
                                    else if(sigstr > 20)
                                                setfillstyle(1,14);
                                                bar(XSTRT-89,YMAX6+34-sigstr,XSTRT-86,(YMAX6+34));
                                    }
                                    else
                                    {
                                                setfillstyle(1,4);
                                                bar(XSTRT-89,YMAX6+34-sigstr,XSTRT-86,(YMAX6+34));
                                    }
                        else if(pad == PAD4 || pad == PAD3)
                                    setfillstyle(0,0);
                                    bar(XSTRT-89,YMAX4+34,XSTRT-86,YMIN4+29);
                                    setfillstyle(1,1);
                                    bar(XSTRT-89,YMAX4+34-sigstr,XSTRT-86,(YMAX4+34));
                        else if(pad == PAD2 || pad == PAD1)
                                    setfillstyle(0,0);
                                    bar(XSTRT-89,YMAX2+34,XSTRT-86,YMIN2+29);
                                    setfillstyle(1,1);
                                    bar(XSTRT-89,YMAX2+34-sigstr,XSTRT-86,(YMAX2+34));
                        delay_sigstr = 0;
            }
}
void draw_rectangles()
            setcolor(7);
           rectangle(XSTRT-90, YMAX8+35, XSTRT-85, YMIN8+28);
rectangle(XSTRT-90, YMAX6+35, XSTRT-85, YMIN6+28);
           rectangle(XSTRT-90, YMAX4+35, XSTRT-85, YMIN4+28);
rectangle(XSTRT-90, YMAX2+35, XSTRT-85, YMIN2+28);
}
void draw_lines()
            setcolor(5);
           line(XSTRT - 25, XAXIS8 + 12, XSTRT - 25, XAXIS7 - 7);
line(XSTRT - 25, XAXIS6 + 12, XSTRT - 25, XAXIS5 - 7);
line(XSTRT - 25, XAXIS6 + 12, XSTRT - 25, XAXIS3 - 7);
            line(XSTRT - 25, XAXIS2 + 12, XSTRT - 25, XAXIS1 - 7);
           line(XSTRT - 25, YMIN7+2, XSTRT - 45, YMIN7+2);
line(XSTRT - 25, YMIN5+2, XSTRT - 45, YMIN5+2);
line(XSTRT - 25, YMIN3+2, XSTRT - 45, YMIN3+2);
line(XSTRT - 25, YMIN1+2, XSTRT - 45, YMIN1+2);
            line(XSTRT-95, YMIN7+2, XSTRT - 115, YMIN7+2);
line(XSTRT-95, YMIN5+2, XSTRT - 115, YMIN5+2);
line(XSTRT-95, YMIN3+2, XSTRT - 115, YMIN3+2);
           line(XSTRT-95, YMIN1+2, XSTRT - 115, YMIN1+2);
            circle(XSTRT - 117, YMIN7+2, 2);
           circle(XSTRT - 117, YMIN5+2, 2);
circle(XSTRT - 117, YMIN3+2, 2);
circle(XSTRT - 117, YMIN3+2, 2);
           setcolor(11);
           arc(XSTRT - 124, YMIN7+2, 90, -90, 4);
arc(XSTRT - 126, YMIN7+2, 90, -90, 6);
arc(XSTRT - 128, YMIN7+2, 90, -90, 8);
           arc(XSTRT - 124, YMIN5+2, 90, -90, 4);
arc(XSTRT - 126, YMIN5+2, 90, -90, 6);
arc(XSTRT - 128, YMIN5+2, 90, -90, 8);
           arc(XSTRT - 124, YMIN3+2, 90, -90, 4);
arc(XSTRT - 126, YMIN3+2, 90, -90, 6);
arc(XSTRT - 128, YMIN3+2, 90, -90, 8);
```





PC Software (Matlab)

function emgdisplay(filename);

% This gives what we want, the proper order for the data. % open file for reading with little-endian byte order FID2 = fopen(filename, 'r', 'l'); % read in 16 bit unsigned values into F2, and count how many values are read in [F2, num_samples] = fread(FID2, inf, 'uint16');

% let 0FFF correspond to +1, and 0 correspond to -1; % scale everything appropriately divide by 0FFF/2 = 2047; scale_fact = 2047; % change this for real code to 2047

 $F3 = (F2/scale_fact) - 1;$

sample_rate = 1000; % sampling rate in Hz time_div = 1/sample_rate; t = 0:time_div:((num_samples - 1)*time_div); % time values to plot samples against

F3T = transpose(F3); % take transpose to match matrix dimensions for plotting
figure; % opens new figure

plot(t, F3,'.',t,F3);

ST2 = fclose(FID2);